PREPARATION AND BIOLOGICAL EVALUATION OF ETHYLCELLULOSE MICROSPHERES CONTAINING TOLMETIN

- Puglisi¹*, G. Giammona¹, N.A. Santagati¹, B. Carlisi² A. Villari³ and S. Spampinato⁴
- Istituto dі Chimica Farmaceutica Tossicologica, е Catania, V.le A. Doria 6, 95125 Catania Università di (Italy).
- Dipartimento Farmaceutiche, dі Chimica e Tecnologie di Palermo, Via Archirafi 32, Università 90132 Palermo (Italy).
- Farmaco-Chimico, Università di Messina, Dipartimento Annunziata, 98010 Messina (Italy).
- Università di di Farmacologia, Bologna. Istituto 48, 40126 Bologna (Italy). Irnerio

ABSTRACT

Tolmetin microspheres were prepared by the coacervation process from the ethylcellulose. Microspheres were obtained both in presence and without protecting colloids, such as polyisobutilene (PIB) or ethyl-vinylacetate copolimers (EVA). The effect of these agents on the preparation, drug content, wall thickness, surface morphology, drug dissolution and re-

^{*}Author to whom correspondence should be submitted.

lease from microspheres, were evaluated. The dissolution rate analysis was carried out also in the presence of a surfactant (Tween 80) at different pH values.

In addition, microspheres containing Tolmetin as a core material were submitted to biological tests, in comparison with the free drug, to evaluate upon experimental models antipyretic activity and the gastric tolerability.

INTRODUCTION

is at present one of the methodolo-Microincapsulation used to control drugs properties. The inclusion of thin particles of a substance in the polymeric wall of microspheres. microscopic sizing packages as containers, lead change the availability of the core material and to alter some of its physical properties, like solubility, chemical reactivity, color, taste and particle shape, besides of tect the core from light, heat and oxidation effects.

Such an ability adds itself, in pharmaceutical formulations, to the possibility of slowing the drug release, well as to prolong its therapeutic activity (1-4).

Many different coating materials and processes can used in the microincapsulation, and several reviews have been published in the last years (5-6).

Tolmetin is a non-steroidal antiinflammatory agent (NSAID) being a pyrrole-acetic acid derivative, which a remarkable analgesic and antiinflammatory efficacy in man (7-9). As well as other NSAIDs, Tolmetin displays a ked irritating effect on gastrointestinal mucosae.



paper reports the preparation of Tolmetin microspheres with ethylcellulose and attemps to observe influence of the use of polyisobutylene or ethylene-vinyl acetate copolymer upon microcapsule size distribution, drug wall thickness, surface morphology and dissolution parameters that control the drug relase rate from the coating polymer. In addition, biological results regarding the activity and tolerability of microencapsulated Tolmetin, with respect to the free drug, are reported.

EXPERIMENTAL SECTION

<u>Materials</u>

obtained as dihydrate sodium salt from Tolmetin was (U.S.A.) and was used as free acid. Ethylcellulose N-Type (Hercules Incorporated, Delaware, USA), has ethoxyl content of 47.5 to 49.0% and the viscosity of a w/w solution in toluene-ethanol (80/20 w/w) was 100 cps. Polyisobutylene (PIB), with a molecular weight of 300.000 was obtained from BASF (Ludwigshafen, Germany) and ethylene-vinyl copolymer (EVA), vinyl acetate content 33%, from acetate (USA). Cyclohexane was of reagent grade. All other Aldrich ingredients and solvents used were of pharmaceutical grade.

Methods

Preparation of the microspheres

preparation was based on the method of Miller al. (10) and Jalsenjak et al. (11). Three hundred milof a cycloexane solution containing Ø or 3% w/w liliters



protective colloid, i.e. PIB or EVA, were placed into a 1 three-necked round-bottomed flask equipedd with a Heidolph mod. RZR 2000 stirrer, a thermometer and a reflux condenser. With stirring at 300 rpm, 0.75g of EC were added at room temperature and the temperature was raised to 66°C over 90 The core material, Tolmetin, was then added (1.5 g) and period of 60 min the temperature was further raised 80°C. After being maintained at this temperature for 60 and with continued stirring, the system was cooled to 35°C in then cooled rapidly with ice to 25°C and stirred 120 for further 20 min. The obtained microspheres were recovered decantation, and the product was washed three times 200 ml aliquots of cyclohexane (10° C), after a 60 min agitathen filtered and air dried overnight. Yields always greater than 95% .

Classification of microspheres

different size of microspheres in the various obtained batches were separated into five fractions sieving on a mechanical shaker using a range of standard sieves $(2000-10000 \, \mu m)$ and a shaking time of $100 \, min$.

Dissolution studies from microspheres

Drug release from microspheres was studied by the tating paddle method specified in F.U.I. (IX Edn.) (12).

Samoles (25 mg) of the selected particle size ranges introduced in different solution media [pH 4 or pH 7.4 and kept at 37± 0.5°C. A stirring (intestinal liquids)]



speed ωf 100 rpm was maintained as constant all experiments. At suitable intervals, a 2 ml aliquot moved and filtered (0.22 μm Millipore membrane). An equivalent quantity of dissolution medium was added into the dissolution vessel immediately after each sample drawing, to mainthe original volume. Dissolution studies were carried tain in the presence of a small amount of surfactant (Tween 80, 0.02%) in order to improve the wetting of spheres.

The concentration of Tolmetin was determined spectrophotometrically at 320 nm. It was confirmed that the surfactant in the medium did not disturb the contained optical absorption of the drug at 320 nm in the present assay.

Dissolution experiments were duplicated and were closely reproducible.

Determination of Microspheres Content

To determine the total drug content in the various fractions of microspheres, 1.25 mg samples were dissolved in 50 ml of methanol, which dissolved off all the coating materials used. The resulting solutions were diluted and assayed spectrophotometrically at 313 nm, using a calibration curve based on standard solutions in methanol.

EC did not absorb in methanol at this wavelenght.

Microscopic Studies

The surface topography of the microspheres were investigated with scanning electron microscopy (SEM). Microcapsule



944

PUGLISI ET AL.

samples were mounted onto stubs using double sided adhesive tape and vacuum-coated with gold film (10 A) by a Polaron Sputter Coater E 5100 and analyzed by a SEM Philips mod. 500 apparatus.

Fluorescence microscopy experiments were carried out by a Reichert-Jung mod. Diastar apparatus, equipped with a exciter filter BG 12 plus KB 418 and a barrier filter DG 515.

Determination of Wall Thickness

The wall thickness of the microspheres was calculated from the drug content, particle size and the relative densities of the wall material and core material. If the particles are assumed to be uniform, smooth and spherical, the average wall thickness is given by Madan's equation [1] (13):

If W≃ weigth of microspheres, Ww is the weight of the wall material, σ is the density the density Tolmetin and d is the mean diameter of drug particles. The density σf the microspheres, the wall (Ethylcellulose) and core material (Tolmetin) were calculated from the displacement volume of a known weight of ethylcellulose and drug using cyclohexane as a displacement fluid by picnometer. The calculated value are 1.11 g/cm 3 for the wall material and 1.75 g/cm ³ for Tolmetin at 25°C.



Biological studies

Animals

Male albino New Zealand rabbits (2.3 ± 0.2 Kg) from Charles River (Calco, Como) were used. Animals were kept in a temperature-controlled room (21 ± 2 °C) with a 12 h light-dark cycle and 60% humidity.

Gastric ulceration assay

Rabbits were fasted overnight and the compounds administered orally as $\emptyset.5\%$ w/v suspensions in carboxymethylcellulose (CMC, 10 ml/Kg).18 h later all the rabbits were sacrificed (sodium pentobarbital, 50 mg/Kg, i.v.). stomach was removed, cut along the greater curvature and lesions on the gastric mucosa counted by visual examination under 3x magnification. All lesions were counted regardless of size. The dose producing gastric lesions in 50%animals (UD₅₀) was determined according to the Litchfield and Wilcoxon (14).

Antipyretic activity

Hyperthermia was induced in rabbits by i.v. injection of μg/kg of bacterial endotoxin from Escherichia Coli, purchased from Sigma Chemical Co (St. Louis, U.S.A.).

Drugs were administered orally in CMC as above, 120 after the injection of pyrogen. Rectal temperature variations was measured at 30 min intervals for 5 h.



RESULT AND DISCUSSION

The preparation of microspheres obtained by coacervation EC as coating material requires a carefull attention details of the procedure in order not to have a containing largely aggregated masses of the starting rials (15). Furthermore, it has been reported the importance of a protective colloid as PIB in forming individually filmcoated core particles as opposed to aggregates we thought to be interesting to study also Moreover, effect of EVA on the preparation of Tolmetin-loaded EC microspheres.

The presence of these agents, like shown by the results causes a decrement in the particle size, Tab.I. remarkable for PIB. Whilst the presence of the coacervating did not significatively influence the drug neither within the different batches nor in the overall microspheres preparation. The coacervation agents were used at a concentration of 3% w/w (8, 20). The wall thickness of the microspheres produced with or without a coacervation-inducing agent increased in the order PIB <none <EVA.

Scanning electron micrographs of microspheres are prein Fig.1 . The surface of the microspheres prepared without any coacervation inducing agent was rough irregular (fig.la).

the case of PIB the surface was smooth, and many small holes were apparent (fig.1b), with EVA, the surface was smooth with a few small holes (fig.1c).



•

Effects of coacervation-inducing agents on microspheres formation.

TABLE I.

_		_		Sie	Sieve fraction (%)	on (%)	
Coacervation	1 Tolmetin	l Wall					
linducing agent 	content (%) 	l thickness l (µm) l	200-355	355-500	588-718 (µm)	500-710 710-1000 (µm)	<1888
None	1 66.7	15.16	19.30	16.00	17.30	20.10	27.30
PIB	1 67.2	1 14.63	23.20	43.60	28.94	3.15	1.11
EVA	1 66.3	15.57	14.06	33.01	29.04	13.14	10.75

3/3 ä, coacervation-inducing agent was The concentration of

ø

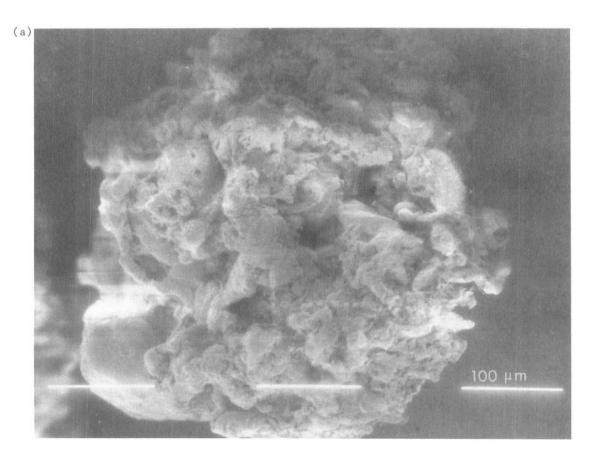


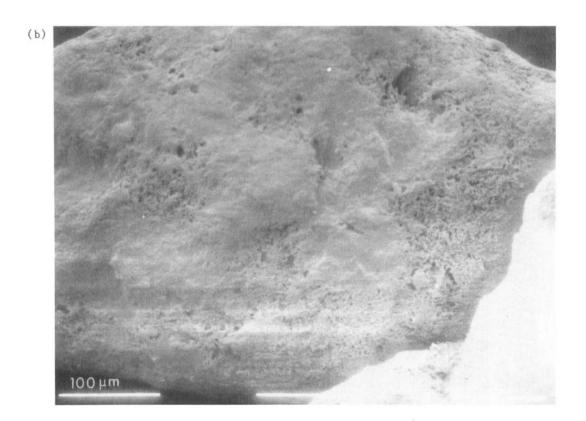
Fig. 1 - Scanning Electron Micrographs of microspheres surfa-

without coacervation-inducing agent, (b) PIB.

(c) EVA.

Findings of SEM analysis can be confirmed by means of fluorescence microscopy (FM). By considering that the drug is fluorescent, unlike EC and coacervating agents, from Fig. 2 it is evident, besides of the occurred coating, that microspheres obtained in the presence of EVA (fig. 2c) reduce more uniformely.





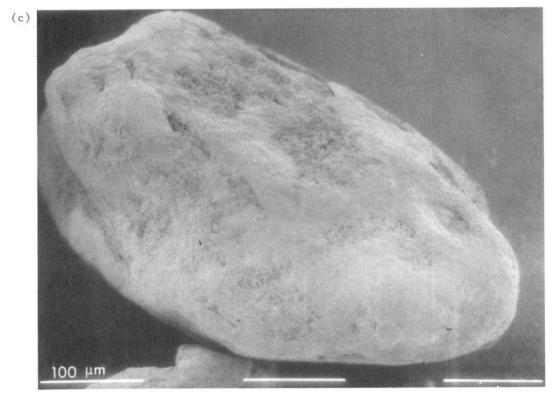


Fig. 1 Continued







Fig. 2 - Fluorescence microscopy of microspheres and uncoated Tolmetin.

- (a) without coacervation-inducing agent, (b) PIB,
- (c) EVA, (d) uncoated Tolmetin.





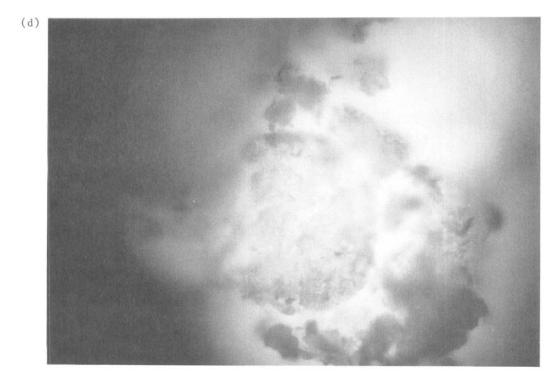


Fig. 2 Continued



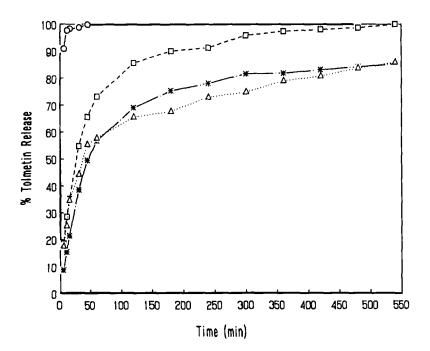
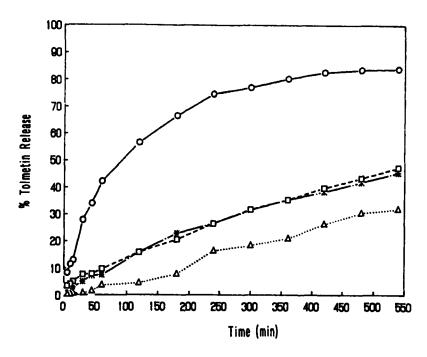


Fig. 3 - Release (%) Tolmetin from microspheres σſ pН temperature of 37 ± a uncoated Tolmetin, $-\Delta$ -: without coacervation inducing agent, -□-: PIB, -#-EVA.

Tolmetin fluorescence (Fig. 2d) with respect to those prepared with PIB or with no coacervating agent, areas with dishomogeneous fluorescence are visible (Fig. 2a). A study on drug dissolution rate was also carried out on EC microspheres, at pH 7.4, in comparison with free drug; the influence of the coacervating agents release from microspheres was in drug the meantime (Fig. 3).

50% οf Tolmetin required to dissolve The (t_{50}) was 37.5 min if the microspheres microspheres were prepared without a coacervation-inducing agent. When PIB





of drug from microspheres at pH 4 at Fig. 4 - Release (%) a temperature of 37 ± 0.1 °C. drug, - 4 -: wi thout uncoated coacervationinducing agent, -O-: PIB, -+-: EVA.

used the t_{50} values were 26.5 and 45.1 EVA were of respectively; unencapsulated Tolmetin showed ^t5Ø about 2.5 min. Changes in t_{50} values are imputable to different wall thichness and uniformity of coating, as SEM and FM. These result are in accordance to Takamura et al. (21), Nixon et al. (22), which ted that the dissolution rate of core material from spheres was related to variables such as wall thickness, rosity, density and other wall characteristics.

verify if dissolution rate of encapsulated influenced by pH variations, we repeated dissolution



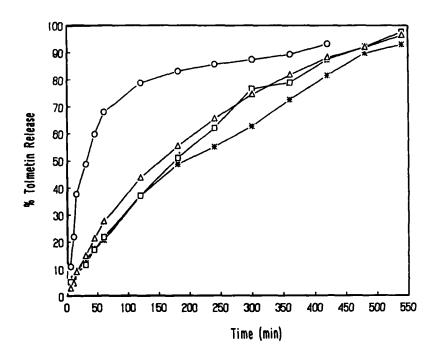


Fig. 5 - Release (%) of Tolmetin from microspheres at pH 4 in at a temperature of presence of Tween 80 (0.02 %) # Ø.1 °C. 37 uncoated Tolmetin, -4-: without inducing agent, -□-: PIB, -♣-: EVA.

tests in a pH 4.0 buffer. Such a pH value was chosen by sidering the insolubility of the drug in a gastric (pH buffer. The analysis at pH 4.0 evidenced a remarkable decreain the percentage of dissolved drug from microspheres regards the values obtained at pH 7.4. These (Fig. 4), as data suggest the suitability of using a surfactant to increase the wettability of microspheres as well as the solubility of the drug in the dissolution medium (23).

The chosen surfactant was Tween 80. The dissolution assays were thus performed again at pH 4.0 and in the presen-



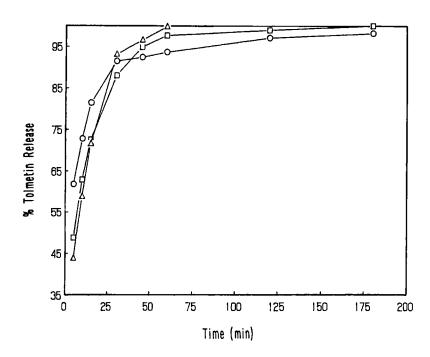


Fig. 6 - Release (%) of drug from microspheres at pH = 7.4 in Tween 80 (0.02%) аt a temperature presence οf ۰C. of 37 ± Ø.1 -Δ-: without coacervation-inducing agent, -D-: -*-: EVA.

ce of 0.02 Tween 80 (Fig. 5). Dissolution rates appeared larenhanced by the surfactant to a t50 of 150.9 the encapsulated Tolmetin (in EC microspheres without any agent) and 37.1 min for the coacervating free drug. Microcapsules obtained in the presence of PIB or EVA t50 values of 172.5 min and 188.6 min, respectively, in theconditions. The influence of tween 80 as the dissolution rate of Tolmetin from microspheres was also verified at In this in presence of PIB and EVA the t_{5Ø} 6.9 and 5.9 min respectively min



956

PUGLISI ET AL,

TABLE II Gastric lesions produced by Tolmetin and microspheres in rabbits after oral administration.

Bitel Dial adi		·	
Compounds	Dose (^a) (mg/Kg)	no. of animals with gastric lesions	
Tolmetin	50 100 200 400	1/6 2/6 3/6 6/6	190 (73-494)
Microspheres(5ø 1øø 2) 2øø 4øø	Ø/6 1/6 2/6 6/6	240 (188-386)
Microspheres(50 100 - 200 400	Ø/6 Ø/6 2/6 5/6	270 (188-386)

in absence of coacervating agent was about 4 min, as shown in Fig. 6.

were Biological tests carried out to the ulcerogenic potency (UD $_{50}$) of Tolmetin carried in microspheres. Results showed that the drug displays a better lerability when it is coated in the microspheres (Table II), as a consequence of the shorter effective contact time with gastric walls.



⁽a) as to the amount of free drug administered.
(b) microspheres without coacervation-inducing agent.
(c) microspheres prepared in the presence of PIB.

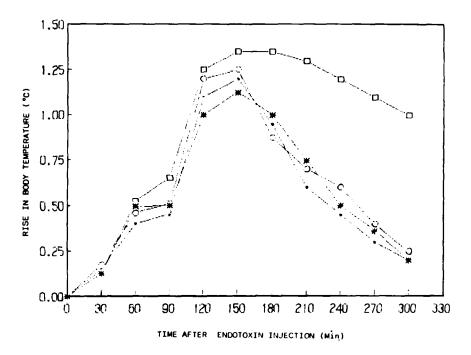


Fig. 7 - Antipyretic activity in rabbit of Tolmetin - 0-, and microspheres prepared without --- or in the preof a coacervation-inducing agent (PIB) rabbits -O-received 10 ml/Kg of 0.5 % W/v Control carboxymethylcellulose time Ø. Each point represents the mean (± S.E.) of 3 rabbits. Standard errors (for values) are not indicated for the several clarity. < Ø.Ø5: ** p < 0.01 vs controls. Student **'** 5 "t" test was used for the of variance.

The slight better value of the ulcerogenic index, in the showed by microspheres prepared presence of a coacervating agent (PIB), night be ascribed to the more uniform of the resulting microspheres, as SEM studies coating showed (Fig.1).

In addition, the antipyretic effect, as reported in Fig. for either Tolmetin or the microspheres prepared



in the presence of a coacervation inducing agent administered orally at a drug dose of 40 mg/Kg, produced a superimposable fall in body temperature rabbits fevered by a bacterial endotoxin-induced pirexia.

ACKNOWLEDGEMENTS

The present work was supported by Italian C.N.R.

REFERENCES

- J. Pharm. Sci., <u>70</u>, 370 (1981). J.R. Nixon,
- N. Leelarasamee, S.A. Howard, C.J. Malanga, L.A. J. Microen-S.J. Kandzari and J.H.K. Ma, T.F. Hogan, capsulation, 3, 171 (1986).
- T. Uchida, I. Fujimoto and S. Goto, Chem. Pharm. Bull., з. 37, 3416 (1989).
- and D.H. Robinson, J. Microencapsulation, 7, J. Singh 4. 67 (1990).
- Illum, J.G. McVie Ε. Tonlinson, s.s. Davis, L. and Microspheres and drug therapy. Pharmaceutical, Immunological and Medical Aspects, Elsevier, 1984.
- C. Washington, Int. J. Pharm., <u>58</u>, 1 (1990).
- S.S. Berkowitz, Curr. Ther. Res., 16, 442 (1974).
- E. Mainbach, Curr. Ther. Res., 19, 350 (1976). 8.
- Bachmann, O. Stroescu and W. Hartl, Therapiewoche, 27, 2262 (1977).
- Miller, G.O. Fanger, and R.G. McNiff, R.E. 10. South Africa pat. 4211-66 (1967).
- Jalsenjak, C.F. Nicolaidou and J.R. Nixon, J.R., J. 11. J. Pharm. Pharmacol., 28, 912 (1976).
- Farmacopea Ufficiale Italiana IX Ed. (1985), Vol. 1, 12. 416
- P.L. Madan, A. Luzzi and J.C. Price, J. Pharm. Sci., 63, 13. 280 (1974).



- F. Wilcoxon, J. Pharmacol. 14. J.T. Litchfield and Ther., 96, 99 (1949).
- R. J. 15. Jalsenjak, J.R. Nixon, Senykovic and Stivic, J. Pharm. Pharmacol., 32, 678 (1980).
- S. Benita and M. Donbrow, J. Colloid Interface Sci., 77, 16. 102 (1980).
- 17. s. Benita and M. Donbrow, J. Pharm. Pharmacol., 77 (1981).
- s. 18. Benita and M. Donbrow, J. Pharm. Sci., 71, 205 (1982).
- 19. M. Donbrow and S. Benita, J. Pharm. Pharmacol., 29, (1977) 4P
- 20. M. Samejima, G. Hirata and Y. Koida, Chem. Bull., <u>30</u>, 2894 (1982).
- K. Takamura, M. Koishi and T. Kondo, J. Pharm. 21. 610 (1973).
- J. R. Nixon 22. and S. E. Walker, J. Pharm. 53 (suppl.), 147S (1971).
- Davis and E. Tomlison, 23. D.J. Burgess, S.S. J. Pharm. 39, 129 (1987).

